Wireless Power Transfer With Zero-Phase-Difference Capacitance Control

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Abstract-Wireless power transfer enables the frequent and ubiquitous charging of electronic devices. However, the variation of the efficiency and the received power with the transmission distance is an outstanding issue. To solve the problem of efficiency degradation of the magnetic resonance at short distances, zero-phase-difference capacitance control (ZPDCC), which is suitable for integration in large scale integrations (LSIs) is proposed in this paper. The proposed ZPDCC achieves adaptive capacitance control by a newly proposed control algorithm with a current-sensing circuit to control variable capacitors at a fixed frequency. Additionally, a theoretical analysis of the total DC-DC power transmission efficiency (η_{TOTAL}) including a power amplifier, coupled resonators, and a rectifier is demonstrated in this paper. The analysis indicates that the frequency (and capacitance) splitting of η_{TOTAL} is mainly due to the power amplifier; additionally, the efficiency of the power amplifier is maximized at the split peaks when the transmission distance (d) is short. A wireless power transfer system in magnetic resonance with ZPDCC is fabricated in a 3.3 V, 180 nm CMOS. By introducing ZPDCC, the measured η_{TOTAL} at 13.56 MHz increases 1.7 times from 16% to 27% at d = 2.5 mm.

Index Terms—Magnetic resonance, power amplifier, wireless power transmission, zero-phase-difference capacitance control.

I. INTRODUCTION

IRELESS power transfer has opened a new era of power distribution without messy wire connections and the inconvenience of charging batteries. Wireless power transfer enables the frequent and ubiquitous charging of electronic devices (e.g., cell phones). However, the transmission efficiency is degraded by radiation loss and the resistive loss of antennas; additionally, the variation of the efficiency and the received power with the transmission distance is also an outstanding issue.

As first proposed in 2007 [1], magnetic resonance has the potential to realize more efficient and stable wireless charging at intermediate distances (1 cm–10 m) than a conventional microwave beam [2] and magnetic induction [3]. Wireless power transmission systems with magnetic resonance consist of a power amplifier, coupled resonators, and a rectifier. The total DC-DC power transmission efficiency (η_{TOTAL}) at the inherent resonant frequency (f_{RES}) of the resonators is maximized at a certain distance, while η_{TOTAL} is reduced at short

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distances (e.g., 1 cm). This efficiency degradation at short distances is a unique phenomenon of magnetic resonance and is not observed in conventional magnetic induction.

To address this issue, several techniques [4]–[20] and theoretical studies [21]-[23] have been reported. Frequency tracking [4]-[9] controls the transmission frequency corresponding to the transmission distance, although frequency deviation is not allowed in many radio bands (e.g., the ISM band [24]). A repeater coil array [10], [11] has a misalignment-tolerant design without frequency deviation; however, the number of transmission coils has to be increased to cover a large misalignment. This increases the size and cost of the transmitter. Supply voltage (V_{DD}) control [12], [13] controls the output power of a power amplifier to regulate the received power, although η_{TOTAL} is greatly reduced by the loss of the DC-DC converter. To address this degradation of efficiency, adaptive impedance matching [14]–[18] has been introduced. The optimum load impedance of a power amplifier has been realized using variable capacitors [15]-[18], while in several studies, a bulky and expensive directional coupler [14], [15] and impedance analyzer [16], [17] were required as detectors.

A theoretical analysis of η_{TOTAL} including a power amplifier, coupled resonators, and a rectifier is newly demonstrated in this paper. The results indicate that the frequency (and capacitance) splitting of η_{TOTAL} is mainly due to the power amplifier and that the efficiency at short distances is maximized at the split peaks. This verifies the effect of zero-phase-difference capacitance control (ZPDCC) [19]. The proposed ZPDCC is suitable for integration in large scale integrations (LSIs) to reduce efficiency degradation of the magnetic resonance at short distances. The proposed ZPDCC achieves adaptive capacitance control by a newly proposed control algorithm with a current-sensing circuit to control variable capacitors at a fixed frequency.

An outline of this paper is given as follows. In Section II, a theoretical analysis of the efficiency degradation of the magnetic resonance at short distances is given. In Section III, a method that increases η_{TOTAL} at short distances without frequency deviation and the need for a bulky detector circuit is proposed. In Section IV, the measured results for a wireless power transfer circuit with ZPDCC are reported. In Section V, conclusions are given.

II. ANALYSIS OF EFFICIENCY OF MAGNETIC RESONANCE

In this section, a theoretical analysis of the efficiency degradation of the magnetic resonance at short distances is given, in particular, the frequency dependence of the efficiency of coupled resonators (η_{RES}) and a power amplifier (η_{PA}) is clarified by theoretical calculations and simulations. These calculations and simulations indicate that frequency splitting is not observed

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in η_{RES} with asymmetric port impedances, while it is observed in η_{PA} . Several studies [4], [7], [15], [16] have investigated the increase in the efficiency between coupled resonators with port impedances of 50 Ω . The efficiency is calculated from $|S_{21}|^2$ measured by a vector network analyzer. However, these studies gave limited conclusions because not only coupled resonators but also a power amplifier made a large contribution to η_{TOTAL} . This study includes a new theoretical analysis of η_{TOTAL} and frequency splitting while taking into account the effect of η_{PA} . In this section, the frequency dependence of η_{TOTAL} with a power amplifier, coupled resonators, and a rectifier is theoretically analyzed to clarify the effect of a power amplifier.

A. Transmission Efficiency Between Coupled Resonators

To analyze the efficiency degradation at short distances and discuss the frequency splitting in the case of asymmetric port impedances, the frequency dependence of η_{RES} is first analyzed. Figs. 1(a) and (b) show a schematic of a wireless power transfer system and the equivalent circuit in magnetic resonance with a power amplifier, coupled resonators, and a rectifier, respectively. V_{DD} is the supply voltage of the power amplifier, $L_{\rm RES}$ is the inductor in each resonator, $C_{\rm RES}$ is the capacitor in each resonator, $C_{\rm L}$ is the load capacitor at the output of the rectifier, $R_{\rm L}$ is a load resistor at the output of the rectifier, k is the coupling coefficient of the coupled resonators, R_{RES} is the equivalent series resistor of the $L_{\text{RES}}, L_{\text{M}}$ is the mutual inductor corresponding to $kL_{\rm RES}$, $V_{\rm IN}$ is the output voltage of the power amplifier, $I_{\rm IN}$ is the output current of the power amplifier, $R_{\rm IN(RECT)}$ is the input resistor of the rectifier, and $Z_{\rm IN}$ is the input impedance of the coupled resonators. Additionally, the input power to the power amplifier, the output power of the power amplifier, the input power to the rectifier, and the load power are denoted as P_1 , P_2 , P_3 , and P_4 , respectively. Then, the efficiency of the power amplifier, coupled resonators, and rectifier, and the total DC-DC power transmission are respectively defined as

$$\eta_{\rm PA} = \frac{P_2}{P_1} \tag{1}$$

$$\eta_{\text{RES}} = \frac{r_3}{P_2} \tag{2}$$

$$\eta_{\text{RECT}} = \frac{I_4}{P_3} \tag{3}$$

$$\eta_{\rm TOTAL} = \eta_{\rm PA} \times \eta_{\rm RES} \times \eta_{\rm RECT} = \frac{P_4}{P_1}.$$
 (4)

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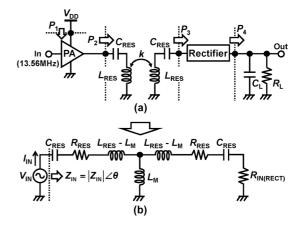


Fig. 1. Schematic of a wireless power transfer system. (a) Block diagram of system with a power amplifier, coupled resonators, and a rectifier. (b) Equivalent circuit.

In previous studies [4], [7], [10], [14]–[17], [23] with a port impedance of 50 Ω , η_{RES} was defined by $|S_{21}|^2$. Integrated wireless power transfer systems are implemented using a digital power amplifier (e.g., class-D [8], [9], [19] or class-E [12], [13], [18], [20]) to maximize η_{PA} and η_{TOTAL} . The output impedance corresponding to the on-resistance of a power transistor is lower than 50 Ω ; additionally, the input impedance of a rectifier varies with the load resistance $(R_{\rm L})$. Therefore, the port impedances of the coupled resonators are not symmetric. A previous theoretical study [21] showed that the frequency splitting of $\eta_{\rm RES}$ is not observed in the case of asymmetric port impedances, while it is observed in the case of symmetric port impedances. This conclusion was obtained by differential calculations of $1/\eta_{\rm RES}$ as shown in [21]. To support the discussions of η_{PA} in the next section, a discussion and findings regarding η_{RES} in the case of asymmetric port impedances are given in this section.

It is first assumed that the coupled resonators of the transmitter and receiver are configured by the same components and that the output impedance of the power amplifier is negligible, compared with the input impedance of the rectifier. Then, η_{RES} in Fig. 1(b) is given by (5), where the Q is the Q factor of the L_{RES} , ω is the angular carrier frequency, and ω_0 is the resonant angular frequency of the L_{RES} and C_{RES} . By differentiating (5) with respect to ω , the angular frequency ($\omega_{\eta \max}$) at the maximum η_{RES} is given by (6). η_{RES} has a maximum value at $\omega_{\eta \max}$, and which means that η_{RES} in the case of asymmetric port impedances does not show frequency splitting. Under the condition $\omega = \omega_{\eta \max}$, the maximum η_{RES} (η_{RESMAX}) is given

$$\eta_{\text{RES}} = \frac{k^2 L_{\text{RES}} Q^3 R_{\text{IN}(\text{RECT})} \omega^4}{k^2 L_{\text{RES}} Q^2 \omega^4 \left(Q R_{\text{IN}(\text{RECT})} + L_{\text{RES}} \omega_0 \right) + \omega_0 \left[2 L_{\text{RES}} Q R_{\text{IN}(\text{RECT})} \omega^2 \omega_0 + L_{\text{RES}}^2 \omega^2 \omega_0^2 + Q^2 \left\{ R_{\text{IN}(\text{RECT})}^2 \omega^2 + L_{\text{RES}}^2 \left(\omega^2 - \omega_0^2 \right)^2 \right\} \right]}$$

$$(5)$$

$$\omega_{\eta \max} = \frac{\sqrt{2} L_{\text{RES}} Q \omega_0^2}{\sqrt{-Q^2} R_{\text{IN}(\text{RECT})}^2 - 2 L_{\text{RES}} Q R_{\text{IN}(\text{RECT})} \omega_0 + L_{\text{RES}}^2 (-1 + 2Q^2) \omega_0^2}$$

$$(6)$$

$$M_{\text{RESMAX}} = \frac{4k^2 L_{\text{RES}}^3 Q^5 R_{\text{IN}(\text{RECT})} \omega_0^3 / \left(Q R_{\text{IN}(\text{RECT})} + L_{\text{RES}} \omega_0 \right)}{-Q^3 R_{\text{IN}(\text{RECT})}^3 - 3 L_{\text{RES}} Q^2 R_{\text{IN}(\text{RECT})}^2 \omega_0 + L_{\text{RES}}^2 Q (-3 + 4Q^2) R_{\text{IN}(\text{RECT})} \omega_0^2 + L_{\text{RES}}^3 (-1 + 4Q^2 + 4k^2 Q^4) \omega_0^3}$$

$$(7)$$

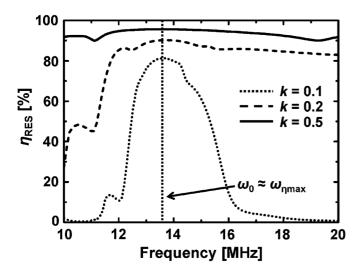


Fig. 2. Simulated frequency dependences of η_{RES} for k = 0.1, 0.2, and 0.5 with the parameters in Table I. The simulations include a power amplifier, coupled resonators, and a rectifier as shown in Fig. 1(a). The simulated frequency dependences of η_{RES} do not show frequency splitting even with the nonlinearity induced by the power amplifier and rectifier.

TABLE I PARAMETERS IN SIMULATIONS

L _{RES}	C _{RES}	$Q(L_{RES})$	$C_{\rm L}$	R _L	V _{DD}
3.3µH	42pF	100	1µF	80Ω	3.3V

by (7) (see equations at bottom of next page). η_{RESMAX} is a monotonically increasing function of k because the derivative of (7) with respect to k is positive for all k excluding k = 0. These results indicate that η_{RES} increases inversely proportionally to the transmission distance without frequency splitting when the port impedances are asymmetric.

Fig. 2 and Table I show the simulated frequency dependences of $\eta_{\rm RES}$ and the parameters used in the simulations, respectively. The parameters in Table I are determined to achieve $P_4 = 50 \text{ mW}$ at a transmission distance and carrier frequency of 30 mm and 13.56 MHz, respectively. The frequency dependences of η_{RES} in Fig. 2 were simulated by SPICE simulation [25] including a power amplifier, coupled resonators, and a rectifier as shown in Fig. 1(a). The simulated result for η_{RES} demonstrates that η_{RES} is maximized at $\omega \approx \omega_0$ and increases with k. This result is consistent with the conclusion that η_{BES} increases inversely proportionally to the transmission distance without frequency splitting. It should be noted that $\omega_{\eta \max}$ is approximately equal to ω_0 when $R_{\rm IN(RECT)}$ is small (e.g., less than 100 Ω under the conditions in Table I), while $\omega_{n \max}$ increases when $R_{IN(RECT)}$ is large. In this study, the deviation of $\omega_{\eta \max}$ is negligible because $R_{\text{IN}(\text{RECT})}$ is small.

B. Frequency Dependence of η_{PA}

The efficiency of the power amplifier is of fundamental importance in a wireless power transfer system because the frequency splitting of η_{TOTAL} is attributed to η_{PA} . Figs. 3(a) and (b) show the Z_{IN} dependences of the output power (P_2) and drain efficiency (η_{PA}) of a power amplifier obtained by a load pull simulation, respectively. P_2 and η_{PA} are fundamentally determined by Z_{IN} . The simulated results show that P_2 and η_{PA}

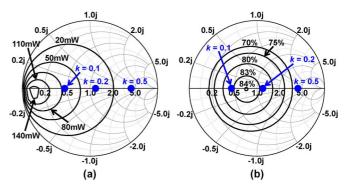


Fig. 3. Z_{IN} dependences of (a) P_2 and (b) η_{PA} for a power amplifier obtained by load pull simulation at 13.56 MHz. Blue dots show the impedances of Z_{IN} for k = 0.1, 0.2, and 0.5 with coupled resonators and a rectifier.

increase when $\operatorname{Re}[Z_{\mathrm{IN}}]$ is decreased and $\operatorname{Im}[Z_{\mathrm{IN}}] = 0$. However, $\operatorname{Re}[Z_{\mathrm{IN}}]$ increases proportionally to k; therefore, P_2 and η_{PA} decrease with increasing k.

To clarify the frequency dependence of the η_{PA} , the frequency dependence of Z_{IN} is theoretically analyzed from the equivalent circuit in Fig. 1(b).

First, $Z_{\rm IN}$ is given by

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$$Z_{\rm IN} = \frac{\omega R_{\rm IN(RECT)} + j L_{\rm RES} \left\{ \left(\omega^2 - \omega_0^2 \right) - \frac{k^2 \omega^4}{\left(\omega^2 - \omega_0^2 \right)} \right\}}{\omega \left(1 - j \frac{R_{\rm IN(RECT)} \omega}{\left(\omega^2 - \omega_0^2 \right) L_{\rm RES}} \right)}$$
(8)

assuming that $R_{\text{RES}} = 0$ for conciseness. Then, $\text{Re}[Z_{\text{IN}}]$ and $\text{Im}[Z_{\text{IN}}]$ are respectively given by

$$\operatorname{Re}[Z_{\mathrm{IN}}] = \frac{k^2 L_{\mathrm{RES}}^2 R_{\mathrm{IN}(\mathrm{RECT})} \omega^4}{R_{\mathrm{IN}(\mathrm{RECT})}^2 \omega^2 + L_{\mathrm{RES}}^2 (\omega^2 - \omega_0^2)^2}$$
(9)
$$\operatorname{Im}[Z_{\mathrm{IN}}] = \frac{R_{\mathrm{IN}(\mathrm{RECT})}^2 \omega^2 + L_{\mathrm{RES}}^2 \left\{ \left(\omega^2 - \omega_0^2\right)^2 - k^2 \omega^4 \right\}}{\frac{R_{\mathrm{IN}(\mathrm{RECT})}^2 \omega^3}{L_{\mathrm{RES}} \left(\omega^2 - \omega_0^2\right)} + L_{\mathrm{RES}} \omega \left(\omega^2 - \omega_0^2\right)}.$$
(10)

Equation (9) shows that $\operatorname{Re}[Z_{\mathrm{IN}}]$ is maximized at $\omega = \omega_0$ and increases proportionally to k^2 . This k dependence of $\operatorname{Re}[Z_{\mathrm{IN}}]$ is also verified in Fig. 3.

To increase P_2 and $\eta_{\rm PA}$, the condition ${\rm Im}[Z_{\rm IN}] = 0$ should be satisfied. When ${\rm Im}[Z_{\rm IN}] = 0$, ω is given by

$$\omega_{\rm LOW} = \sqrt{\frac{1 + \sqrt{1 + \frac{4(-1+k^2)L_{\rm RES}^2\omega_0^4}{\left(R_{\rm IN(RECT)}^2 - 2L_{\rm RES}^2\omega_0^2\right)^2}}{\frac{2(-1+k^2)L_{\rm RES}^2}{R_{\rm IN(RECT)}^2 - 2L_{\rm RES}^2\omega_0^2}}, \quad (11)$$

$$\omega_{\text{CENTER}} = \omega_0, \tag{12}$$

$$\omega_{\rm HIGH} = \sqrt{\frac{1 - \sqrt{1 + \frac{4(-1+k^2)L_{\rm RES}^4\omega_0^4}{\left(R_{\rm IN(RECT)}^2 - 2L_{\rm RES}^2\omega_0^2\right)^2}}{\frac{2(-1+k^2)L_{\rm RES}^2}{R_{\rm IN(RECT)}^2 - 2L_{\rm RES}^2\omega_0^2}}.$$
 (13)

where ω_{LOW} , ω_{CENTER} , and ω_{HIGH} are a low value of ω , an intermediate value of ω corresponding to ω_0 , and a high value of ω with $\text{Im}[Z_{\text{IN}}] = 0$, respectively. Equations (11) and (13) are only valid when k satisfies

$$k > \frac{1}{2} \sqrt{\frac{-R_{\rm IN(RECT)}^4 + 4L_{\rm RES}^2 R_{\rm IN(RECT)}^2 \omega_0^2}{L_{\rm RES}^4 \omega_0^4}}.$$
 (14)

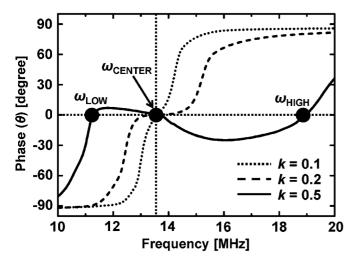


Fig. 4. Simulated frequency dependences of phase between $V_{\rm IN}$ and $I_{\rm IN}$ for k = 0.1, 0.2, and 0.5 with the parameters in Table I. The simulation includes a power amplifier, coupled resonators, and a rectifier. Black dots show $\omega_{\rm LOW}$, $\omega_{\rm CENTER}$, and $\omega_{\rm HIGH}$ given by (11)–(13) for k = 0.5. $V_{\rm IN}$ and $I_{\rm IN}$ are defined as shown in Fig. 1(b) and are equivalent to the output voltage and output current of the power amplifier, respectively. The phase is defined as the delay of $I_{\rm IN}$ relative to $V_{\rm IN}$ at ω_0 ; ω at ${\rm Im}[Z_{\rm IN}] = 0$ and $\theta = 0$ are equivalent because the frequency dependence of ${\rm Im}[Z_{\rm IN}]$ corresponds approximately to that of θ .

This means that there are three solutions ($\omega = \omega_{\text{LOW}}$, ω_{CENTER} , and ω_{HIGH}) satisfying $\text{Im}[Z_{\text{IN}}] = 0$ when the transmission distance is short, while there is only one solution ($\omega = \omega_{\text{CENTER}}$) when the transmission distance is long.

Fig. 4 shows the simulated frequency dependences of the phase (θ) between the input voltage ($V_{\rm IN}$) and input current ($I_{\rm IN}$) to the coupled resonators in Fig. 1(b). The simulated frequency dependences of θ demonstrate that $\theta = 0$ only at $\omega = \omega_0 (= \omega_{\rm CENTER})$ when k = 0.1 and 0.2, while $\theta = 0$ at $\omega = \omega_0$, $\omega_{\rm LOW}$, and $\omega_{\rm HIGH}$ when k = 0.5. This verifies the results of analysis using (11)–(14).

To increase P_2 and $\eta_{\rm PA}$, a smaller $\operatorname{Re}[Z_{\rm IN}]$ with $\theta = 0$ should be used when the transmission distance is short. The expressions for $\operatorname{Re}[Z_{\rm IN}]$ at $\omega = \omega_{\rm LOW}$, $\omega_{\rm CENTER}$, and $\omega_{\rm HIGH}$ are given by

$$\operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{LOW}})\right] = \operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{HIGH}})\right] = R_{\mathrm{IN}(\mathrm{RECT})}$$
(15)

$$\operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{CENTER}})\right] = \frac{k^2 L_{\mathrm{RES}}^2 \omega_0^2}{R_{\mathrm{IN}(\mathrm{RECT})}}.$$
(16)

Then, the relationships among $\operatorname{Re}[Z_{IN}]$ at $\omega = \omega_{LOW}$, ω_{CENTER} , and ω_{HIGH} are given by

$$\operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{LOW}})\right] = \operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{HIGH}})\right] < \operatorname{Re}\left[Z_{\mathrm{IN}}(\omega_{\mathrm{CENTER}})\right]. \quad (17)$$

Equation (17) indicates that P_2 and $\eta_{\rm PA}$ at $\omega = \omega_{\rm LOW}$ and $\omega_{\rm HIGH}$ are larger than those at $\omega = \omega_{\rm CENTER}$ because ${\rm Re}[Z_{\rm IN}]$ at $\omega = \omega_{\rm LOW}$ and $\omega_{\rm HIGH}$ is smaller than that at $\omega = \omega_{\rm CENTER}$ when the transmission distance is short. It should be noted that P_2 and $\eta_{\rm PA}$ at $\omega = \omega_{\rm LOW}$ are higher than those at $\omega = \omega_{\rm HIGH}$ because the power dissipation induced by switching loss and $R_{\rm RES}$ due to the skin effect increase in proportion to the frequency.

Fig. 5 shows the simulated frequency dependences of η_{PA} . When k = 0.1 and 0.2, η_{PA} is maximized at $\omega = \omega_{\text{CENTER}}$, while η_{PA} is maximized at $\omega = \omega_{\text{LOW}}$ and ω_{HIGH} when k

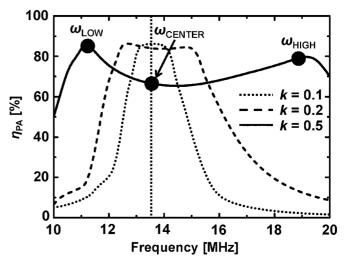


Fig. 5. Simulated frequency dependences of $\eta_{\rm PA}$ for k = 0.1, 0.2, and 0.5 with the parameters in Table I. The simulation includes a power amplifier, coupled resonators, and a rectifier. Black dots show $\omega_{\rm LOW}$, $\omega_{\rm CENTER}$, and $\omega_{\rm HIGH}$ given by eqs. (11)–(13) for k = 0.5.

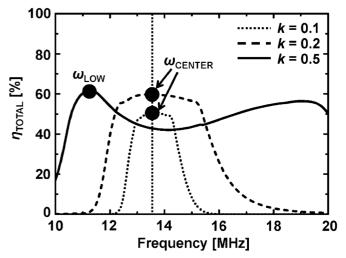


Fig. 6. Simulated frequency dependences of η_{TOTAL} for k = 0.1, 0.2, and 0.5 with the parameters in Table I. The simulation includes a power amplifier, coupled resonators, and a rectifier. Black dots show ω for the maximum η_{TOTAL} at each k.

= 0.5. ω with the maximum $\eta_{\rm PA}$ at each distance in Fig. 5 corresponds to the points satisfying $\theta = 0$ at $\Delta\theta/\Delta\omega > 0$ in Fig. 4. This means that ω should be controlled under the condition $\theta = 0$ at $\Delta\theta/\Delta\omega > 0$ depending on the transmission distance in order to maximize $\eta_{\rm PA}$. Using this modified ω , $\eta_{\rm PA}$ is maximized even with the frequency splitting of $\eta_{\rm PA}$ when the transmission distance is short.

C. Frequency Dependences of η_{RECT} and η_{TOTAL}

 η_{RECT} increases proportionally to P_3 which corresponds to the output power of the power amplifier; therefore, the frequency dependences of η_{RECT} correspond approximately to that of η_{PA} .

Fig. 6 shows the simulated frequency dependences of η_{TOTAL} . Since η_{TOTAL} is the product of η_{PA} , η_{RES} , and η_{RECT} , η_{TOTAL} also exhibits frequency splitting when the transmission distance is short. The maximum efficiency is achieved at $\omega = \omega_{\text{CENTER}}$ when k = 0.1 and 0.2, while η_{TOTAL} is maximized at $\omega = \omega_{\text{LOW}}$ when k = 0.5.

III. ZERO-PHASE-DIFFERENCE CAPACITANCE CONTROL

The origin of the frequency splitting of η_{TOTAL} in a wireless power transfer system was explained in the previous section. However, adaptive frequency control ($\theta = 0$ at $\Delta \theta / \Delta \omega$ > 0) is not permitted in many radio bands. In this study, the lower peak of η_{TOTAL} is moved from ω_{LOW} to a fixed target frequency ($\omega_{\text{TARGET}} = 13.56 \text{ MHz}$) by changing C_{RES} in order to increase η_{TOTAL} at short distances for the fixed frequency of 13.56 MHz. Conventional studies [15]-[18] on capacitance control require bulky and expensive detectors because these algorithms for capacitance control must detect S_{11} [15] or $Z_{\rm IN}$ [16], [17]. On the other hand, the proposed algorithm of zero-phase-difference capacitance control (ZPDCC) only requires the phase (θ) between V_{IN} and I_{IN} for the coupled resonators in Fig. 1(b). This means that the proposed ZPDCC achieves efficient implementation in a small space using a current monitor, which is easily implemented into integrated circuits.

The duality between the capacitance dependence and the frequency dependence is given by substituting

$$\omega_0 = \frac{1}{\sqrt{L_{\text{RES}}C_{\text{RES}}}} \tag{18}$$

in (8)–(17). In particular, capacitance splitting corresponding to $\theta = 0$ at a fixed frequency ($\omega_{\text{TARGET}} = 13.56 \text{ MHz}$) is observed at

$$C_{\rm LOW} = \frac{L_{\rm RES} - \sqrt{k^2 L_{\rm RES}^2 - \frac{R_{\rm L}^2}{\omega_{\rm TARGET}^2}}}{R_{\rm L}^2 + L_{\rm RES}^2 \omega_{\rm TARGET}^2 (1 - k^2)},$$
 (19)

$$C_{\text{CENTER}} = \frac{1}{L_{\text{RES}}\omega_{\text{TARGET}}^2},$$
(20)

$$C_{\rm HIGH} = \frac{L_{\rm RES} + \sqrt{k^2 L_{\rm RES}^2 - \frac{R_{\rm L}^2}{\omega_{\rm TARGET}^2}}}{R_{\rm L}^2 + L_{\rm RES}^2 \omega_{\rm TARGET}^2 (1 - k^2)}.$$
 (21)

Fig. 7 shows simulated capacitance dependences of the phase (θ) between $V_{\rm IN}$ and $I_{\rm IN}$ for the coupled resonators in Fig. 1(b). Similarly to the previous section, $\eta_{\rm TOTAL}$ is maximized at $C_{\rm RES} = C_{\rm LOW}$ and $C_{\rm HIGH}$ with capacitance splitting when the transmission distance is short, while it is maximized at $C_{\rm RES} = C_{\rm CENTER}$ at longer distances. In ZPDCC, the appropriate $C_{\rm RES}$ is searched for under the condition $\theta = 0$ at $\Delta\theta/\Delta C > 0$. This condition determines whether the transmission distance is short or long.

Fig. 8 shows a flow chart of the proposed algorithm for ZPDCC. To compensate for the offset of θ caused by parasitic capacitances and the delay of the current monitor, this algorithm requires calibrations of the capacitance before and after shipment. Details of the proposed algorithm are given below.

- A) Calibrations before shipment
 - 1) To compensate for parasitic capacitance and inductance on the PCB and mismatches in fabrication, the $C_{\text{RES}}[i]$ corresponding to the maximum η_{TOTAL} is searched for by the hill climbing method when the transmission distance is sufficiently long.
 - 2) The obtained $C_{\text{RES}}[i]$ is assigned as the initial value of C_{RESINIT} . C_{RESINIT} results in the maximum η_{TOTAL} at ω_{TARGET} when the capacitance splitting of η_{TOTAL} is not observed.

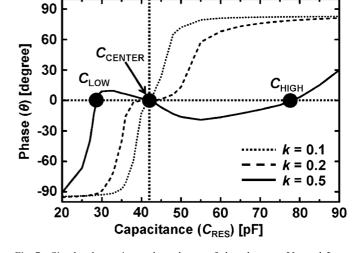


Fig. 7. Simulated capacitance dependences of phase between $V_{\rm IN}$ and $I_{\rm IN}$ at $\omega_{\rm TARGET} = 13.56$ MHz for k = 0.1, 0.2, and 0.5 with the parameters in Table I excluding $C_{\rm RES}$. The simulation includes a power amplifier, coupled resonators, and a rectifier. Black dots show $C_{\rm LOW}$, $C_{\rm CENTER}$, and $C_{\rm HIGH}$ given by (19)–(21) for k = 0.5.

- B) Calibrations after shipment
 - 3) θ is measured at the calibrated C_{RESINIT} and the measured θ is assigned as the initial value of θ_{INIT} . In the proposed ZPDCC, the difference between θ and θ_{INIT} is used to discriminate whether the transmission distance is short or large. In ZPDCC, the lower peak is searched for because fewer capacitor banks are required than for a search for the higher peak. Therefore, the capacitance is finally reduced from i to i-1.
 - 4) θ is measured at the reduced C_{RES} corresponding to i-1 and the measured θ is compared with θ_{INIT} .
 - 5) When the measured θ is smaller than θ_{INIT} , the condition $\theta = 0$ at $\Delta \theta / \Delta C > 0$ is satisfied in ZPDCC without capacitance splitting. This means that the transmission distance is large and that C_{RESINIT} should be used as the modified C_{RES} (C_{RESMOD}).
 - 6) When the measured θ is larger than θ_{INIT} , the transmission distance is short and capacitance splitting is observed. Therefore, C_{RESMOD} should be searched for and set to C_{LOW} . In this process, θ is repeatedly measured and compared while reducing C_{RES} until the condition $\theta \leq \theta_{\text{INIT}}$ is satisfied.
 - 7) When the measured θ is equal to θ_{INIT} , C_{RES} corresponds to C_{LOW} ; therefore, C_{RES} is assigned to C_{RESMOD} .
 - 8) When the measured θ is less than θ_{INIT} , the resolution of the capacitor bank is larger than the resolution of the phase detector. To prevent the over tune of C_{RES} , $C_{\text{RES}}[i + 1]$ is assigned to C_{RESMOD} .

Fig. 9 shows simulated capacitance dependences of η_{TOTAL} for k = 0.1, 0.2, and 0.5. Capacitance splitting is only observed for k = 0.5. Using the proposed ZPDCC, C_{RES} is determined so that the maximum η_{TOTAL} is achieved, which depends on the transmission distance. When k = 0.1 and $0.2, \theta = 0$ only at C_{CENTER} , then, using the proposed ZPDCC, it is found that $C_{\text{RESMOD}} = C_{\text{RESINIT}} = C_{\text{CENTER}}$ as shown in Fig. 8 (case 5). On the other hand, $\theta = 0$ at $C_{\text{LOW}}, C_{\text{CENTER}}$, and C_{HIGH} when k = 0.5, then, using the proposed ZPDCC, it is found

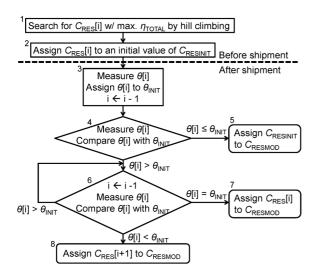


Fig. 8. Flow chart of algorithm of ZPDCC. C_{RESMOD} denotes C_{RES} modified by ZPDCC. In this algorithm, it is assumed that C_{RES} is digitally controlled. The digital code of C_{RES} is given by the integer value i.

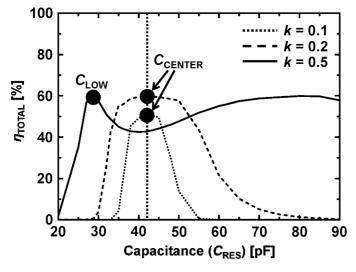


Fig. 9. Simulated capacitance dependences of η_{TOTAL} for k = 0.1, 0.2, and 0.5 with the parameters in Table I excluding C_{RES} . The simulation includes a power amplifier, coupled resonators, and a rectifier. Black dots show C_{RESMOD} corresponding to the maximum η_{TOTAL} for each k, which is determined by ZPDCC.

that $C_{\text{RESMOD}} = C_{\text{LOW}}$ as shown in Fig. 8 (case 7 or 8). The modified C_{RESMOD} gives the maximum η_{TOTAL} for each k as shown in Fig. 9.

IV. MEASUREMENT RESULTS AND DISCUSSION

To demonstrate the improvement of η_{TOTAL} upon using the proposed ZPDCC, a wireless power transfer system in magnetic resonance with the ZPDCC is implemented. Fig. 10 shows a circuit schematic of the wireless power transfer system in magnetic resonance with the ZPDCC. The class-D PA in the transmitter and the rectifier in the receiver are designed and fabricated in a 3.3 V, 180 nm CMOS process. The L_{RES} are fabricated on an FR4 PCB and the layout of the L_{RES} is the same as that in [10]. The capacitors on the PCB are implemented by ceramic capacitors.

In the circuit implementation of ZPDCC, θ is measured as the phase difference between the voltage (V_1) and current (I_1) in the transmitter. I_1 is converted to a voltage by a non-inverting amplifier, which is implemented using an operational amplifier

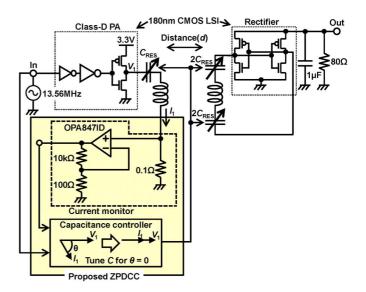


Fig. 10. Circuit schematic of wireless power transfer system in magnetic resonance with ZPDCC. All the simulation results in this paper are shown on this schematic.

(OPA847ID [26]) and two resistors. The gain of the amplifier is set to $1 + (10 \text{ k}\Omega/100 \Omega) = 40 \text{ dB}$. In the measurement, the phase difference θ between V_1 and I_1 is measured by an oscilloscope, and the capacitance is changed by manually replacing the ceramic capacitors with a minimum resolution of 0.5 pF. The capacitance is tuned in accordance with the flow chart in Fig. 8.

To achieve automated control, the implementation of a phase detector, capacitance controller, and communication link between the transmitter and receiver is required for the integration of LSIs. First, the phase detector could be implemented in the LSIs using a time-to-digital converter (TDC) with a resolution of 20 ps ($\approx 0.1^{\circ}$ at 13.56 MHz) and 290 pJ/conversion-step [27]. The digitized phase data from the TDC is input to the capacitance controller (= state machine corresponding to the algorithm of ZPDCC), and the capacitance controller controls the 7-bit binary capacitor bank. The capacitor bank could be tuned by relays [15], [28] in the range of 15-45 pF on the transmitter and 30-90 pF on the receiver with a minimum resolution of 0.5 pF. In high-power applications, the on-resistance of the switches reduces η_{TOTAL} if V_{DD} is not scaled in accordance with the transmission power. The large current flow in the switches consumes a huge amount of power. On the other hand, the power consumption in the switches is not increased if $V_{\rm DD}$ is increased using high-voltage technologies (e.g., LDMOS and IGBT) depending on the transmission power. Such high-voltage technologies would realize highly efficient implementation with capacitance control even in high-power applications. Additionally, the on-resistance of the switches ($\approx 0.2 \Omega$ [28]) is smaller than $R_{\rm RES} (\approx 3 \Omega)$. This implies that the loss due to the on-resistance is not dominant in the whole system. Finally, the communication link between the transmitter and receiver could be implemented by backscattering [29], [30]. Wireless communication at 6.78 Mbps [30] without any extra antennas has been reported. The capacitor bank on the receiver is controlled in accordance with the received data. This whole system, which includes a current monitor, phase detector, capacitance controller, and communication link, is easily implemented into integrated circuits. Compared with conventional capacitance control methods

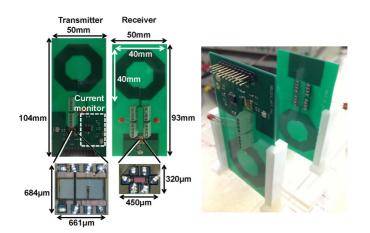


Fig. 11. Photographs of transmitter and receiver on PCB, LSIs of PA and rectifier, and measurement equipment.

TABLE II $L_{\text{RES}}, R_{\text{RES}}$, and Q Factor of L_{RES} Obtained by EM Simulation and Measurement

	$L_{\rm RES}$ [µH]	$R_{\rm RES} \left[\Omega \right]$	Q factor
EM Simulation	3.38	2.90	96
Measurement	3.42	2.67	109

using a directional coupler [15] and a vector network analyzer [16], [17], ZPDCC is more suitable for the integration in LSIs.

Fig. 11 shows photographs of the transmitter and receiver in the wireless power transfer system in magnetic resonance. The LSIs of the PA and rectifier, and the measurement equipment are also shown in Fig. 11. The size of the L_{RES} fabricated on the PCB in the transmitter and receiver is 40 mm × 40 mm. The core sizes of the PA and rectifier are 684 μ m × 661 μ m and 320 μ m × 450 μ m, respectively.

Table II shows a comparison of L_{RES} , R_{RES} , and the Q factor of the L_{RES} obtained by EM simulation and measurement at 13.56 MHz. The measurement results are in good agreement with the values in Table I. This means that the simulated results in previous sections and the measurement results are consistent.

Fig. 12 shows a comparison of $|S_{21}|$ for coupled resonators at transmission distances (d) of 5 mm, 15 mm, and 25 mm obtained by EM simulation and measurement. The measurement results are consistent with the simulated results and frequency splitting at d = 5 mm is observed.

Fig. 13 shows the simulated transmission distance dependence of the coupling coefficient (k) at 13.56 MHz. This result shows that the parameters (k = 0.1, 0.2, and 0.5) used in previous sections approximately correspond to d = 5 mm, 15 mm, and 25 mm, respectively.

Fig. 14 shows the measured frequency dependences of η_{TOTAL} at d = 5 mm, 15 mm, and 25 mm. When d = 15 mm and 25 mm, the frequency dependences of η_{TOTAL} do not exhibit frequency splitting; therefore, η_{TOTAL} is maximized at 13.56 MHz. In contrast, the frequency dependence of η_{TOTAL} at d = 5 mm exhibits frequency splitting. η_{TOTAL} at d = 5 mm is maximized at the lower peak corresponding to ω_{LOW} .

Fig. 15 shows the measured capacitance dependences of θ at 13.56 MHz when d = 5 mm, 15 mm, and 25 mm. When d = 15 mm and 25 mm, $\theta = 0$ once, which corresponds to $C_{\text{CENTER}}(= 37 \text{ pF})$ with the maximum η_{TOTAL} . In contrast,

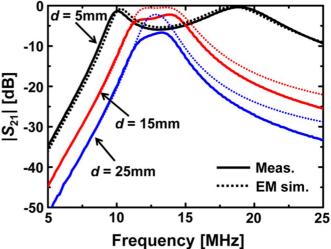


Fig. 12. EM-simulated and measured frequency dependences of $|S_{21}|$ in coupled resonators at transmission distances (d) of 5 mm, 15 mm, and 25 mm.

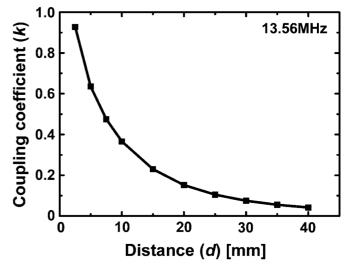


Fig. 13. Simulated transmission distance dependence of coupling coefficient (k) at 13.56 MHz.

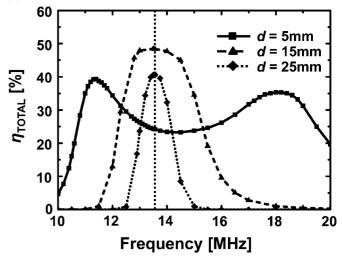


Fig. 14. Measured frequency dependences of η_{TOTAL} at $C_{\text{RES}} = 37 \text{ pF}$ when d = 5 mm, 15 mm, and 25 mm.

when d = 5 mm, $\theta = 0$ at C_{LOW} and C_{CENTER} . C_{RES} is modified from $C_{\text{CENTER}}(= 37 \text{ pF})$ to $C_{\text{LOW}}(= 25 \text{ pF})$ by the proposed ZPDCC with the condition $\theta = 0$ at $\Delta\theta/\Delta C > 0$

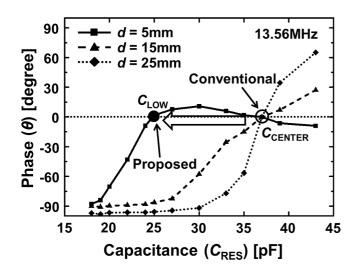


Fig. 15. Measured capacitance dependences of θ at 13.56 MHz when d = 5 mm, 15 mm, and 25 mm. θ is measured by an oscilloscope.

when the transmission distance is short (d = 5 mm). The relay switches should have an operation time of 1 ms [28] to 5 ms [15] and be the slowest block in the automated ZPDCC. The maximum iteration step is determined at the minimum transmission distance. At the minimum distance of 2.5 mm, the capacitor is tuned from 37 pF to 20 pF with a minimum step of 0.5 pF. This corresponds to 35 steps and a settling time of less than 200 ms.

Fig. 16 shows the measured capacitance dependences of η_{TOTAL} at 13.56 MHz when d = 5 mm, 15 mm, and 25 mm. When d = 15 mm and 25 mm, η_{TOTAL} is maximized at C_{CENTER} of 37 pF. In contrast, η_{TOTAL} at d = 5 mm is maximized at C_{LOW} of 25 pF. Using the proposed ZPDCC, η_{TOTAL} is increased from 25% to 34% with the capacitance control of C_{RES} from $C_{\text{CENTER}} (= 37 \text{ pF})$ to $C_{\text{LOW}} (= 25 \text{ pF})$. The measured load power (P_4) at d = 5 mm is also increased from 4.8 mW to 8.4 mW. The maximum P_4 of 56 mW is achieved at d = 30 mm. On the other hand, the measured $\eta_{\rm TOTAL}$ at d = 5 mm is lower than the simulated η_{TOTAL} owing to the coarse minimum resolution of $C_{\text{RES}}(= 0.5 \text{ pF})$ and the mismatches of C_{RES} between the transmitter and receiver. η_{TOTAL} at short distances will be increased if the fine minimum resolution of C_{RES} and a calibration method between the transmitter and receiver are realized.

Fig. 17 shows the measured transmission distance (d) dependence of η_{TOTAL} at 13.56 MHz. The conventional constant capacitance method and the proposed ZPDCC are compared. When d is longer than 10 mm, ZPDCC does not modify C_{RES} from C_{CENTER} . Therefore, η_{TOTAL} for the proposed ZPDCC and the conventional constant capacitance method would be equivalent under ideal conditions. In the measurement, however, η_{TOTAL} for ZPDCC is 1–7% lower than that for the conventional constant capacitance method because of the resistive loss of 0.1 Ω for the current monitor shown in Fig. 10. In contrast, when d is less than 10 mm, η_{TOTAL} for ZPDCC is higher than that for the conventional constant capacitance method, which indicates that the increase in η_{TOTAL} caused by ZPDCC exceeds the decrease in η_{TOTAL} caused by the resistive loss. For example, η_{TOTAL} increases 1.7-times from 16% to 27% at d = 2.5 mm upon tuning C_{RES} from 37 pF to 20 pF. In ZPDCC, the maximum η_{TOTAL} is 49% at d = 15 mm.

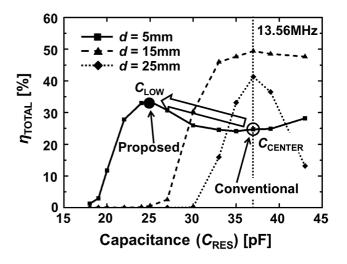


Fig. 16. Measured capacitance dependences of η_{TOTAL} at 13.56 MHz when d = 5 mm, 15 mm, and 25 mm.

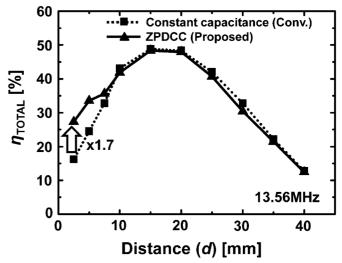


Fig. 17. Measured distance dependences of η_{TOTAL} using conventional constant capacitance method and proposed ZPDCC at 13.56 MHz.

Table III shows a comparison with the results for previously reported wireless power transfer systems at a fixed frequency. At a fixed frequency, only $V_{\rm DD}$ control [13] and impedance matching [15] target the efficiency degradation. This work is the first report of capacitance control including a power amplifier and a rectifier; additionally, the directional coupler used in the previous impedance-matching method is not required. The $V_{\rm DD}$ control method does not include the loss of the DC-DC converter. The efficiency of the corresponding state-of-the-art DC-DC converter is 60–85% in the voltage range 0.6–2.5 V [31]. This implies that the efficiency of the previous $V_{\rm DD}$ control method is greatly reduced by the low efficiency of the DC-DC converter.

V. CONCLUSION

In this paper, zero-phase-difference capacitance control (ZPDCC), which is suitable for integration in LSIs was proposed to solve the problem of efficiency degradation of the magnetic resonance at short distances. The proposed ZPDCC achieves adaptive capacitance control by a newly proposed control algorithm in which $\theta = 0$ at $\Delta\theta/\Delta C > 0$ with a current-sensing circuit to control variable capacitors at a fixed

\$85%

49%

	Control method	Frequency	TX-RX coil diameter	$R_{ m L}$	Max. η_{TOTAL}	Distance at max. η_{TOTAL}	Load Power at max. η_{TOTAL}
[13]	$V_{\rm DD}$ control	6.785MHz	30-30mm	$10 \mathrm{k} \Omega$	[†] 74%	2mm	10mW

 50Ω

80Ω

300-300mm

40-40mm

TABLE III COMPARISON WITH RESULTS FOR PREVIOUSLY REPORTED WIRELESS POWER TRANSFER SYSTEMS AT FIXED FREQUENCY

[†]DC-DC converter is not included. [‡]PA and rectifier are not included.

13.56MHz

13.56MHz

[†]DC-DC converter is not included. [‡]PA and rectifier are not included.

Impedance matching

ZPDCC

[15]

This work

frequency. Additionally, a theoretical analysis of η_{TOTAL} including a power amplifier, coupled resonators, and a rectifier was demonstrated in this paper. A wireless power transfer system in magnetic resonance with ZPDCC is fabricated in a 3.3 V, 180 nm CMOS. By introducing ZPDCC, the measured η_{TOTAL} at an f_{RES} of 13.56 MHz increases 1.7-times from 16% to 27% at d = 2.5 mm.

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REFERENCES

- A. Kurs, A. Karalis, R. Moffatt, J. D. Joannopoulos, P. Fisher, and M. Soljacic, "Wireless power transfer via strongly coupled magnetic resonances," *Science*, vol. 317, pp. 83–86, Jul. 2007.
- [2] W. C. Brown, "Experiments in the transportation of energy by microwave beam," in *Proc. IRE Int. Convention Rec.*, Mar. 1964, vol. 12, pp. 8–17.
- [3] G. Jong and B. Cho, "An energy transmission system for an artificial heart using leakage inductance compensation of transcutaneous transformer," *IEEE Trans.Power Electron.*, vol. 13, no. 6, pp. 1013–1022, Nov. 1998.
- [4] A. P. Sample, D. A. Meyer, and J. R. Smith, "Analysis, experimental results, range adaptation of magnetically coupled resonators for wireless power transfer," *IEEE Trans. Ind. Electron.*, vol. 58, no. 2, pp. 544–554, Feb. 2011.
- [5] D. Ahn and S. Hong, "A transmitter or a receiver consisting of two strongly coupled resonators for enhanced resonant coupling in wireless power transfer," *IEEE Trans. Ind. Electron.*, vol. 61, no. 3, pp. 1193–1203, Mar. 2014.
- [6] D. Ahn and S. Hong, "Wireless power transmission with self-regulated output voltage for biomedical implant," *IEEE Trans. Ind. Electron.*, vol. 61, no. 5, pp. 2225–2235, May 2014.
- [7] J. Park, Y. Tak, T. Kim, Y. Kim, and S. Nam, "Investigation of adaptive matching methods for near-field wireless power transfer," *IEEE Trans. Antennas Propag.*, vol. 59, no. 5, pp. 1769–1773, May 2011.
- [8] Q. Chen, S. C. Wong, C. K. Tse, and X. Ruan, "Analysis, design, control of a transcutaneous power regulator for artificial hearts," *IEEE Trans. Biomed. Circuits Syst.*, vol. 3, no. 1, pp. 23–31, Feb. 2009.
- [9] A. J. Moradewicz and P. Kazmierkowski, "Contactless energy transfer system with FPGA-controlled resonant converter," *IEEE Trans. Ind. Electron.*, vol. 57, no. 9, pp. 3181–3190, Sep. 2010.

[10] K. Mori, H. Lim, S. Iguchi, K. Ishida, M. Takamiya, and T. Sakurai, "Positioning-free resonant wireless power transmission sheet with staggered repeater coil array (SRCA)," *IEEE Antennas Wireless Propag. Lett.*, vol. 11, pp. 1710–1713, 2012.

150mm

15mm

6.8W

24mW

- [11] Y. Narusue, Y. Kawahara, and T. Asami, "Impedance matching method for any-hop straight wireless power transmission using magnetic resonance," in *Proc. IEEE RWS*, Jan. 2013, pp. 20–23.
- [12] G. Wang, W. Liu, M. Sivaprakasam, and G. A. Kendir, "Design and analysis of an adaptive transcutaneous power telemetry for biomedical implants," *IEEE Trans. Circuits Syst. I, Reg. Papers*, vol. 52, no. 10, pp. 2109–2117, Oct. 2005.
- [13] M. W. Baker and R. Sarpeshkar, "Feedback analysis and design of RF power links for low-power bionic system," *IEEE Trans. Biomed. Circuits Syst.*, vol. 1, no. 1, pp. 28–38, Mar. 2007.
- [14] Y. Moriwaki, T. Imura, and Y. Hori, "Basic study on reduciton of reflected power using DC/DC converters in wireless power transfer system via magnetic resonant coupling," in *Proc. IEEE INTELEC*, Oct. 2011, pp. 1–5.
- [15] T. C. Beh, M. Kato, T. Imura, S. Oh, and Y. Hori, "Automated impedance matching system for robust wireless power transfer via magnetic resonance coupling," *IEEE Trans. Ind. Electron.*, vol. 60, no. 9, pp. 3689–3698, Sep. 2013.
- [16] K. Sasaki, S. Sugiura, and H. Iizuka, "Distance adaptation method for magnetic resonance coupling between variable capacitor-loaded parallel-wire coils," *IEEE Trans. Microw. Theory Tech.*, vol. 62, no. 4, pp. 892–900, Apr. 2014.
- [17] K. Ogawa, N. Oodachi, S. Obayashi, and H. Shoki, "A study of efficiency improvement of wireless power transfer by impedance matching," in *Proc. IEEE IMWS-IWPT*, May 2012, pp. 155–157.
- [18] E. M. Thomas, J. D. Heebl, C. Pfeiffer, and A. Grbic, "A power link study of wireless non-radiative power transfer systems using resonant shielded loops," *IEEE Trans. Circuits Syst. I, Reg. Papers*, vol. 59, no. 9, pp. 2125–2136, Sep. 2012.
- [19] S. Iguchi, P. Yeon, H. Fuketa, K. Ishida, T. Sakurai, and M. Takamiya, "Zero phase difference capacitance control (ZPDCC) for magnetically resonant wireless power transmission," in *Proc. IEEE WPTC*, May 2013, pp. 25–28.
- [20] J. J. Casanove, Z. N. Low, and J. Lin, "Design and optimization of a class-E amplifier for a loosely coupled planar wireless power system," *IEEE Trans. Circuits Syst. II, Exp. Briefs*, vol. 56, no. 11, pp. 830–834, Nov. 2009.
- [21] I. Awai and T. Ishizaki, "Transferred power and efficiency of a coupledresonator WPT system," in *Proc. IEEE IMWS-IWPT*, May 2012, pp. 105–108.
- [22] J. L. Villa, J. Sallan, J. F. S. Osorio, and A. Llombart, "High-misalignment tolerant compensation topology for ICPT systems," *IEEE Trans. Ind. Electron.*, vol. 59, no. 2, pp. 945–951, Feb. 2012.
- [23] N. Inagaki, "Theory of image impedance matching for inductively coupled power transfer systems," *IEEE Trans. Microw. Theory Tech.*, vol. 62, no. 4, pp. 901–908, Apr. 2014.
- [24] "Frequency allocations of amateur satellite service," Article 5, 5.150, ISM applications, ITU [Online]. Available: http://www.itu.int/en/ITU-R/space/AmateurDoc/ARS-ART5_E.pdf
- [25] Virtuoso Multi-Mode Simulation With SPECTRE Platform, Spectre RF Datasheet, Cadence Design Systems, Inc. [Online]. Available: http://www.cadence.com/rl/Resources/datasheets/virtuoso_mmsim.pdf#page=4
- [26] Wideband, Ultra-Low Noise, Voltage Feedback Operational Amplifier, OPA847ID Datasheet, Texas Instruments [Online]. Available: http:// www.ti.com/lit/ds/symlink/opa847.pdf

- [27] R. B. Staszewski, S. Vemulapalli, P. Vallur, J. Wallberg, and P. T. Balsara, "1.3 V 20 ps time-to-digital converter for frequency synthesis in 90-nm CMOS," *IEEE Trans. Circuits Syst. II, Ex. Briefs*, vol. 53, no. 3, pp. 220–224, Mar. 2006.
- [28] Reed relay, D31B3100 Datasheet, Celduc Relais [Online]. Available: http://www.celduc-relais.com/all/pdfcelduc/D31B_1_0.pdf
- [29] X. Li, C. Tsui, and W. Ki, "A 13.56 MHz wireless power transfer system with reconfigurable resonant regulating rectifier and wireless power control for implantable medical devices," in *IEEE Symp. VLSI Circuits Dig. Tech. Papers*, Jun. 2014, pp. 28–29.
- [30] S. Ha, C. Kim, J. Park, S. Joshi, and G. Cauwenberghs, "Energy-recycling integrated 6.78-Mbps data 6.3-mW power telemetry over a single 13.56 MHz inductive link," in *IEEE Symp. VLSI Circuits Dig. Tech. Papers*, Jun. 2014, pp. 66–67.
- [31] L. G. Salem and P. P. Mercier, "An 85%-efficiency fully integrated 15-ratio recursive switched-capacitor DC-DC converter with 0.1-to-2.2 V output voltage range," in *IEEE Int. Solid-State Circuits Conf. Dig. Tech. Papers*, Feb. 2014, pp. 88–89.



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